

## 1 Aerodynamic Particle Size Measurement for Inhalation Liquid Preparations

(吸入液剤の空気力学的粒度測定法)

This test is used to evaluate the fine particle characteristics of the aerosol generated by a nebulizer from inhalation liquid preparations<sup>1,2)</sup>.

### 1. Apparatus

The tests are usually performed using the apparatus 3 in Aerodynamic Particle Size Measurement for Inhalations <6.15>, calibrated at a flow rate of 15 L per minute. For the critical dimensions and validation of the apparatus (stage mensuration), also refer to Aerodynamic Particle Size Measurement for Inhalations <6.15>. As inhalation liquid preparations should be evaluated at a flow rate lower than the range typically used for dry powder inhalers and metered-dose inhalers, a flow rate of 15 L per minute is recommended. This is based on the typical breathing volume for an adult (500 mL). To quantitatively collect droplets discharged at 15 L per minute, a back-up filter is used in addition to a micro-orifice collector (MOC). The back-up filter is located below the MOC (internal filter option) or using an external filter holder, to collect any fine droplets that pass through the final stage (MOC). A pre-separator is not used to evaluate droplets generated by a nebulizer.

### 2. Points to consider in the test

#### 2.1 Prevention of evaporation

Controlling the evaporation of droplets produced by a nebulizer is important to avoid bias in the droplet size evaluation process. Evaporation can be minimized by cooling an apparatus to about 5°C, so cool an apparatus in a refrigerator (at about 5°C) for about 90 minutes beforehand<sup>3)</sup>.

#### 2.2 Over-discharging into the apparatus

In the development and validation of the test method, it should be confirmed that the amount of liquid discharged from a nebulizer is not excessive for the apparatus. If over-discharging does occur, a streaky pattern on the surface of the collection stage can be visually confirmed. This phenomenon is usually associated with an increase in the amount of drug collected at the final stage and the back-up filter. To avoid over-discharging and balance discharged amount and analytical sensitivity, it is most effective to shorten the sampling time ( $T_0$ ).

#### 2.3 Mass balance (Recovery rate of drugs)

Because of the continuous discharge of drugs from inhalation liquid preparations, it is not easy to evaluate mass balance in the same way as for dry powder inhalers and metered-dose inhalers. Recovery experiments should be conducted as the part of the method development and validation.

#### 2.4 Re-entrainment

Droplets discharged from a nebulizer are less likely to bounce or be re-entrained than solid inhalation particles, so coating the surface of a collection cup is not usually necessary.

### 2.5 Cleaning of apparatus

The apparatus should usually be thoroughly cleaned, including the inter-stage passageways, at least after each day of use. This is to prevent the corrosion of the metal parts between the stages due to condensation/accumulation of droplets containing salts that occur when the apparatus is cooled. All surfaces of the apparatus should be dried by an appropriate method (e.g., compressed air) after cleaning. However, MOC should not be dried with compressed air.

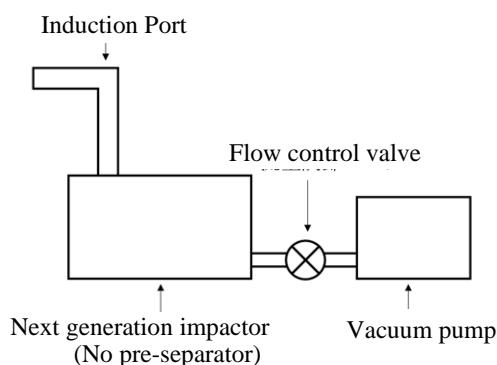
### 3. Test procedures

#### 3.1 Preparation

Cool the apparatus and the induction port in a refrigerator (at about 5°C) for more than 90 minutes beforehand. Other methods that can measure while cooling an apparatus at a constant temperature (e.g., use of a cooling cabinet) can be used, if no difference in the results of particle size distribution is validated.

Prepare a nebulizer according to the patient instructions. Fill the nebulizer with a dose of the drug solution according to the dosage and administration of the inhalation liquid preparation to be measured.

Take out the apparatus from the refrigerator. Attach the induction port to the apparatus, and connect the outlet of the apparatus/external filter to a vacuum pump that is capable of drawing air through the apparatus at 15 L per minute, as shown in Fig.1. Connect a flowmeter, calibrated for the volumetric flow leaving the meter, to the induction port. Run the pump, and adjust the flow control valve between the apparatus and the pump to achieve a steady flow of 15 L per minute ( $\pm 5\%$ ). Then, remove the flowmeter from the apparatus.



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**Fig. 1** Configuration of a next generation impactor for the aerodynamic particle size measurement of inhalation liquid preparations

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#### 3.2. Measurement

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90 Start measurements within 5 minutes after taking out the  
 91 apparatus from a refrigerator. Connect the mouthpiece of a  
 92 nebulizer to the induction port in the same direction as when  
 93 used by patients. Use a mouthpiece adapter if necessary.  
 94 Switch on a nebulizer. After collecting drugs for the prede-  
 95 fined sampling time ( $T_0$ ) so that the mass fraction can be cal-  
 96 culated, switch off the nebulizer. Remove the nebulizer from  
 97 the induction port, and switch off the pump. Dismantle the  
 98 apparatus and determine the amounts of active substance col-  
 99 lected in the induction port, all stages, and the back-up filter  
 100 using a suitable method of analysis, as directed under Aero-  
 101 dynamic Particle Size Measurement for Inhalations <6.15>.  
 102 Drugs collected in the MOC and the back-up filter/external  
 103 filter are combined and treated as a single sample.

#### 104 4. Calculation

105 Calculate the fine particle mass per the specified sampling  
 106 time ( $T_0$ ). Calculate the mass fraction ( $F_{m,comp}$ ) of active sub-  
 107 stance collected at each stage in the apparatus, in order from  
 108 the induction port, using the following equation:

$$109 F_{m,comp} = m_{comp} / M$$

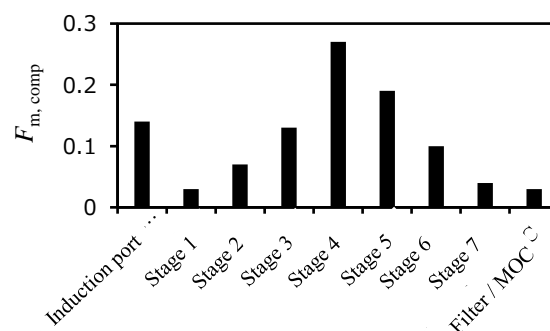
110  $m_{comp}$  = Mass of active substance collected at each stage

111  $M$  = Total mass of active substance collected from the ap-  
 112 paratus

113 Arrange  $F_{m,comp}$  in order of location within the apparatus,  
 114 beginning at the induction port and ending with the back-up  
 115 filter (Fig. 2). If multiple stages are reported as a single value  
 116 due to grouping, the  $F_{m,comp}$  values for adjacent stages may be  
 117 combined.

118 Calculate the cumulative fraction of active substance of  
 119 droplets mensurated by the apparatus as directed under Aer-  
 120 odynamic Particle Size Measurement for Inhalations <6.15>.  
 121 Starting at the filter, calculate the cumulative mass of the ac-  
 122 tive substance versus the cut-off diameter of each stage (see  
 123 Table 1 for the appropriate cut-off diameters of the apparatus  
 124 3 at 15 L per minute<sup>4</sup>). Plot the cumulative fraction of the  
 125 active substance versus the cut-off diameter on an appropri-  
 126 ate graph, e.g., a logarithmic graph or a log-probability graph.  
 127 If necessary, this plot can be used to determine the fraction  
 128 below a given size or between the upper and lower limits of  
 129 size by interpolation.

130 The plot can also be used to determine the mass median  
 131 aerodynamic diameter (MMAD) and geometric standard de-  
 132 viation (GSD).



134 **Fig. 2** Example of mass fraction of active substance col-  
 135 lected at each stage

136 **Table 1** Cut-off diameters of the apparatus 3 when used at  
 137 a flow rate of 15 L per minute

Stage	Cut-off diameter ( $\mu\text{m}$ )
1	14.1
2	8.61
3	5.39
4	3.30
5	2.08
6	1.36
7	0.98

#### 138 5. References

- 139 1) European Pharmacopoeia 11.0 (2022), 2.9.44. Prepara-  
 140 tions for Nebulisation: Characterisation.
- 141 2) US Pharmacopeia (2023), <1601> Products for Nebuli-  
 142 zation - Characterization Tests.
- 143 3) E. Berg, et al., J. Aerosol Med., 20, 97-104 (2007).
- 144 4) V.A. Marple, et al., J. Aerosol Med., 17, 335-343 (2004).